

Accepted Manuscript

Fast laboratory-based micro-computed tomography for pore-scale research: illustrative experiments and perspectives on the future

Tom Bultreys , Marijn A. Boone , Matthieu N. Boone ,
Thomas De Schryver , Bert Masschaele , Luc Van Hoorebeke ,
Veerle Cnudde

PII: S0309-1708(15)00106-2
DOI: [10.1016/j.advwatres.2015.05.012](https://doi.org/10.1016/j.advwatres.2015.05.012)
Reference: ADWR 2384



To appear in: *Advances in Water Resources*

Received date: 19 March 2015
Revised date: 12 May 2015
Accepted date: 13 May 2015

Please cite this article as: Tom Bultreys , Marijn A. Boone , Matthieu N. Boone , Thomas De Schryver , Bert Masschaele , Luc Van Hoorebeke , Veerle Cnudde , Fast laboratory-based micro-computed tomography for pore-scale research: illustrative experiments and perspectives on the future, *Advances in Water Resources* (2015), doi: [10.1016/j.advwatres.2015.05.012](https://doi.org/10.1016/j.advwatres.2015.05.012)

This is a PDF file of an unedited manuscript that has been accepted for publication. As a service to our customers we are providing this early version of the manuscript. The manuscript will undergo copyediting, typesetting, and review of the resulting proof before it is published in its final form. Please note that during the production process errors may be discovered which could affect the content, and all legal disclaimers that apply to the journal pertain.

1 Highlights

- 2 • State of the art in fast laboratory-based X-ray micro-computed tomography is outlined
- 3 • Real-time, pore-scale visualization of drainage in Bentheimer with lab-based scanner
- 4 • Solute transport is imaged at the pore scale in a limestone at 12 seconds per scan

5

ACCEPTED MANUSCRIPT

6 Fast laboratory-based micro-computed tomography for pore-scale research:
7 illustrative experiments and perspectives on the future

8 Tom Bultreys^a, Marijn A. Boone^{a,b}, Matthieu N. Boone^c, Thomas De Schryver^c, Bert Masschaele^{b,c}, Luc
9 Van Hoorebeke^c and Veerle Cnudde^a

10

11 ^aUGCT/PProGress, Dept. of Geology and Soil Science, Ghent University, Krijgslaan 281 (S8), 9000,
12 Ghent, Belgium

13 ^bX-Ray Engineering bvba, De Pintelaan 111, 9000 Ghent, Belgium

14 ^cUGCT/Radiation Physics, Dept. of physics and astronomy, Ghent University, Proeftuinstraat 86, 9000
15 Ghent, Belgium

16

17 **Corresponding author:**

18 Tom Bultreys
19 Dept. of Geology and Soil Science/Centre for X-ray Tomography (UGCT), Ghent University
20 Krijgslaan 281 (S8)
21 9000 Ghent
22 Belgium
23 Tom.Bultreys@UGent.be
24 Tel: +32(0)9 264 46 33
25

26

27

28

29

30

31

32

33

34

35

36

37

38

39

40

41 Key points

42 -The current state of the art in fast (sub-minute) laboratory-based X-ray micro-computed tomography is
43 outlined

44 -Drainage in Bentheimer is visualized in real time at the pore scale with a laboratory-based scanner

45 -Solute transport of a tracer salt is imaged at the pore scale in a limestone sample at 12 seconds per scan

46

47 Abstract.

48 Over the past decade, the wide-spread implementation of laboratory-based X-ray micro-computed
49 tomography (micro-CT) scanners has revolutionized both the experimental and numerical research on
50 pore-scale transport in geological materials. The availability of these scanners has opened up the
51 possibility to image a rock's pore space in 3D almost routinely to many researchers. While challenges do
52 persist in this field, we treat the next frontier in laboratory-based micro-CT scanning: in-situ, time-
53 resolved imaging of dynamic processes. Extremely fast (even sub-second) micro-CT imaging has become
54 possible at synchrotron facilities over the last few years, however, the restricted accessibility of
55 synchrotrons limits the amount of experiments which can be performed. The much smaller X-ray flux in
56 laboratory-based systems bounds the time resolution which can be attained at these facilities.

57 Nevertheless, progress is being made to improve the quality of measurements performed on the sub-
58 minute time scale. We illustrate this by presenting cutting-edge pore scale experiments visualizing two-
59 phase flow and solute transport in real-time with a lab-based environmental micro-CT set-up. To outline
60 the current state of this young field and its relevance to pore-scale transport research, we critically
61 examine its current bottlenecks and their possible solutions, both on the hardware and the software level.
62 Further developments in laboratory-based, time-resolved imaging could prove greatly beneficial to our
63 understanding of transport behavior in geological materials and to the improvement of pore-scale
64 modeling by providing valuable validation.

65

66 Keywords

67 4D micro-computed tomography, dynamic imaging, pore scale, drainage, solute transport

68

69

70

71

72

73

74

75

76 **Manuscript**77 **1 GENERAL INTRODUCTION**

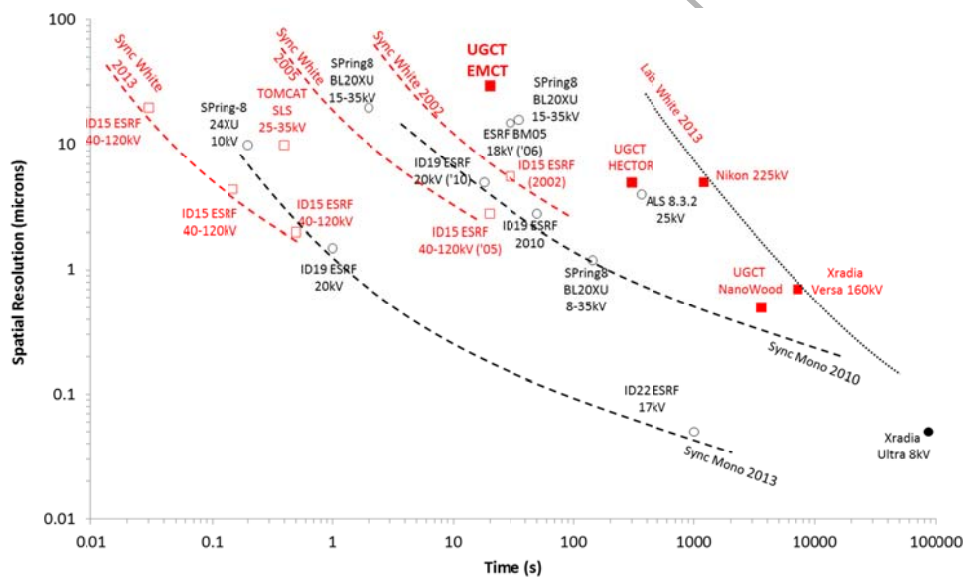
78 Understanding how fluids migrate through porous rocks and how this affects the minerals inside that rock
79 is essential in numerous geological applications, going from the formation and weathering of geological
80 materials (e.g. building stones) to the production and storage of fluids in geological reservoirs. Although
81 fluid migration influences the behavior of these geological materials on the macroscopic scale (meter to
82 kilometer scale for building stones and geological reservoirs, respectively), the essential flow and
83 alteration processes occur on the pore scale (nanometer to micrometer scale), between the minerals of the
84 porous geological material. Comprehending the underlying pore scale processes is crucial to make
85 accurate predictions and decisions regarding important challenges like CO₂-sequestration, environmental
86 remediation of polluted aquifers, enhanced oil recovery and cultural heritage preservation. Of particular
87 interest in this regard are multi-phase and multi-component (reactive) fluid flow, and the coupling of
88 mechanical deformation or failure of the material of interest with such flow phenomena.

89 Understanding the pore scale behavior which controls these processes, however, is a difficult problem
90 which requires three-dimensional pore space characterization. Pore spaces in geological materials often
91 have a complex microstructure, which can span the centimeter to the nanometer scale and can be very
92 heterogeneous in nature. Therefore, their characterization requires more than experiments which measure
93 global information like porosity and pore size distribution. Three-dimensional imaging techniques fill this
94 requirement by providing local geometrical and topological information. The most mature experimental
95 technique in this category is X-ray micro-computed tomography (micro-CT) [1,2]. Before, researchers
96 either had to extrapolate two-dimensional measurements to obtain pseudo-three-dimensional volume
97 information or perform laborious serial sectioning experiments to obtain such local information. Micro-
98 CT however allows the non-destructive visualization of internal pore space structures in three dimensions.
99 The recent increase in the availability of laboratory-scale micro-CT instrumentation has enabled many
100 researchers to characterize the pore space of geomaterials in 3D on an almost routine basis, although a
101 number of limitations in both the acquisition and the analysis of micro-CT data persist. For example, the
102 attainable spatial resolution is often on the order of 1 to a few microns and depends on the size of the
103 studied sample, while the acquisition time is typically on the order of 30 minutes to a few hours.

104 While 3D pore space characterization is an essential part of any pore scale transport or degradation study,
105 it does not provide insight into the dynamics of the processes under investigation. To avoid image
106 blurring (and other motion artifacts), the imaged sample should remain unchanged during the micro-CT
107 acquisition. Therefore, there is a need for fast, time-resolved 3D (i.e. 4D) imaging of a material's
108 microstructure while such a process is taking place, as the only alternative is imposing quasi-static
109 conditions by halting the process during every imaging experiment [3]. Extremely fast micro-CT imaging
110 has become available at synchrotrons over the last few years, attaining even a sub-second time resolution
111 [2–5]. Although a comprehensive review of dynamic experiments performed at synchrotrons is out of the
112 scope of this article, we mention some notable examples of pore scale imaging (in a geological context) at
113 the sub-minute time scale of two-phase flow [6–9] and reactive flow [10]. Other examples of fast imaging
114 of porous media at synchrotron institutions can be found in [11–13]. While synchrotron experiments are
115 proving very valuable, the restricted accessibility of synchrotrons limits the amount of experiments which
116 can be performed. Therefore, the development of laboratory-based fast (sub-minute) micro-CT scanning
117 can prove important, as it would drastically increase the availability of 4D imaging with sub-minute time
118 resolutions. Fast lab-based micro-CT would also allow researchers to prepare 4D experiments in the lab

119 before performing them with higher temporal or spatial resolutions and with better image quality at a
 120 synchrotron. This would be of high value to help optimize the use of synchrotron beam time.

121 Despite the desirability of fast lab-based micro-CT, the much smaller X-ray flux in lab-based systems
 122 bounds the time resolution which can be attained. Just like an underexposed photograph appears noisy
 123 due to photon counting statistics, the restriction on the X-ray flux in laboratory sources limits the image
 124 quality for short acquisition times. Other complications which may occur are for example insufficient
 125 angular sampling, too long detector read-out times and limited rotation speed. Despite the fact that rather
 126 little attention has been given to this topic in the literature (with the exception of work performed by
 127 researchers at the Australian National University [14–16]), advances in micro-CT hardware and in
 128 reconstruction and analysis software are starting to render sub-minute pore-scale experiments possible at
 129 laboratory set-ups. In this work, we illustrate this by the visualization of drainage of a Bentheimer
 130 sandstone and convective/diffusive mass transport of a salt (CsCl) in a water-saturated Savonnières
 131 limestone. In both experiments, the acquisition time per full micro-CT scan was 12 seconds, with a voxel
 132 size of 14.8 μm . While, naturally, the data quality is not as good as what can be expected from similar
 133 experiments performed at synchrotrons, we show that the obtained quality is sufficient to visualize many
 134 interesting aspects of the investigated transport processes in individual pores, even without applying
 135 special reconstruction algorithms. To our knowledge, the experiments reported in this work are the fastest
 136 in-situ, lab-based pore-scale micro-CT measurements of this kind described in the literature until now.
 137 Figure 1 illustrates the progress in attainable spatial and temporal resolution in micro-CT over the years,
 138 both at synchrotron and in typical laboratory-sources [3].



139
 140 **Figure 1.** This figure (adapted from [3]) shows temporal and spatial resolutions attained at different
 141 synchrotron beamlines and lab set-ups. Open symbols denote synchrotron sources, while filled ones
 142 represent laboratory sources, squares denote polychromatic (“white”) beam and circles denote
 143 monochromatic scanners. In cases where the spatial resolution is not cited, an estimated resolution of
 144 twice the voxel size is used. We follow this convention to report the spatial resolution in our own
 145 experiments. The reported time is the time needed to gather 1000 projections.

146 Given the importance of the development of fast 4D lab-based micro-CT to the pore scale modeling and
 147 experimentation community, we describe the current state of the art and the expected future development

148 of this field. Note, however, that this work is not intended as a comprehensive review but rather aims to
149 provide a concise outline of the current and future possibilities of this experimental technique. In section
150 2, we discuss the optimization of various hardware and software components. In section 3.1, we show the
151 real-time imaging of drainage at the pore scale in a Bentheimer sandstone, and in section 3.2 the imaging
152 of advective-diffusive mass transport of a tracer salt in a water-saturated limestone is presented. These
153 experiments simultaneously illustrate the use of fast 4D lab-based tomography in pore scale experiments
154 and the current state of the art of this method.

155 **2 TECHNOLOGICAL ADVANCES**

156 In order to obtain a high-quality micro-CT scan, the accumulated X-ray dose in the detector during the
157 acquisition of the projection images has to be sufficiently high, as the signal-to-noise ratio varies
158 approximately as the square root of the amount of photons which hit the detector. In laboratory-based
159 micro-CT systems, this sets a lower limit to the acquisition time, as the used X-ray flux emitted by the X-
160 ray source is typically low (taking into account also the necessary minimum distance between the source
161 and the detector, due to considerations regarding image magnification, sample size and cone beam
162 artifacts). The limitations of these sources with respect to dynamic imaging are explained in section 2.1.1,
163 as well as technological developments which might mitigate these limitations in the future. Other
164 limitations on the image acquisition may be posed by the X-ray detector (section 2.1.2). During dynamic
165 experiments on porous materials, the sample conditions are usually controlled in some way (e.g. applying
166 mechanical loading, imposing (reactive) fluid flow, controlling temperature and humidity). Therefore, the
167 sample usually has to be contained in a cell or a similar set-up. These cells can affect the image quality,
168 and should therefore be designed carefully (section 2.1.3).

169 After treating the hardware challenges, we discuss the possibilities of smart image reconstruction and
170 analysis to compensate for low image quality (section 2.2). Fast scans, acquired while dynamic processes
171 are going on in the pore space, can and should be supplemented with as much prior information as
172 possible. In many experiments, prior information about the pore geometry can be acquired with a long,
173 high-quality scan while the sample is in static conditions. Other prior information might pertain to the
174 dynamic process itself, for example, in immiscible two-phase flow experiments the assumptions of
175 incompressible fluids and the presence of only three material phases can improve reconstructions with a
176 limited number of projections [14]. By scanning faster, the quality will typically decrease, hence
177 approaches using a priori information gain importance. Another principle which we expect will prove
178 important in the future, is the incorporation of the time dimension in the image analysis. On the one hand,
179 there is a need for software tools which allow researchers to track changes in their sample over time (e.g.
180 deformation of a sample, velocities of fluid interfaces) and help them to make sense of the typically huge
181 amount of data they acquire during a dynamic experiment. On the other hand, truly treating micro-CT
182 time series data as 4D datasets may improve image analysis results, as it allows to incorporate more
183 information. However, one thing is certain: 4D data analysis is computationally intensive, both when it
184 comes to data storage as processing. Section 2.2.2 treats these challenges and opportunities.

185 **2.1 HARDWARE EVOLUTIONS**

186 **2.1.1 X-ray Sources**

187 X-ray sources in laboratory-based micro-CT set-ups are typically microfocus X-ray tubes, in which an
188 electron beam is focused on a very small focal spot on the anode target. When the electrons hit the target
189 after being accelerated by a high-voltage electric field, they create X-rays through their interaction with

190 the anode material. The main limitation of laboratory-based micro-CT in the scope of fast image
191 acquisition is posed by the X-ray source. Unlike synchrotron sources, which exhibit very high brilliance,
192 traditional laboratory sources have a limited X-ray output due to the power dissipation limitation when
193 the electrons hit the anode target, implying longer acquisition times. Indeed, the energy efficiency of X-
194 ray production in the form of Bremsstrahlung in this set-up is only about 1%, and a large portion of
195 electron beam energy is deposited as heat. The power density limit of approximately $2\text{W}/\mu\text{m}^2$ in the target
196 is close to the fundamental limit at which material vaporization starts taking place, despite efforts of
197 rotating anode systems [2]. As a result, the maximum achievable X-ray flux in laboratory systems is
198 strongly correlated with the achieved focal spot size, and hence inversely correlated to the achievable
199 image resolution. This resolution is important to resolve a pore space with sufficient detail (typical
200 geological pore-scale micro-CT studies employ resolutions of 1^3 to $20^3 \mu\text{m}^3$ with acquisition times
201 increasing strongly for higher resolutions, see Figure 1).

202 Recently, the invention of the liquid metal-jet X-ray source has mitigated the power density limit in
203 laboratory X-ray sources. In this set-up, the anode target is a thin jet of liquid metal, hence renewing the
204 target material constantly to avoid vaporization. The liquid metal-jet tubes are commonly used for X-ray
205 diffraction (e.g. [17,18]), but have also proven their value for high-resolution X-ray imaging [19–22]. For
206 the imaging of pore-scale dynamics, their applicability can be limited by the lower limit of the focal spot
207 size (approximately 5-6 μm) and the low energy of the generated X-rays, caused by the low atomic
208 numbers of the materials used as liquid metal. Recently, a setup using Indium (characteristic $K\alpha$ energy
209 24.2 keV) has also been used for hard X-ray imaging [23,24]. When spatial resolutions better than 5-6 μm
210 (hence smaller focal spot sizes) are required, transmission-type X-ray tubes need to be used. Nowadays,
211 several manufacturers offer transmission targets on diamond substrate, allowing for an improved heat
212 dissipation as compared to conventional beryllium substrates. Nevertheless, the highest achievable output
213 power is relatively low due to the absence of direct, active cooling of the target.

214 Other alternative X-ray sources are based on inverse Compton-scattering [25,26]. While such sources
215 may become more accessible in the future, they are not treated here in detail as they are currently still
216 under development and not yet commercially available on a large scale.

217 2.1.2 X-Ray Detectors

218 Due to the limited X-ray flux achievable with conventional laboratory-based sources, image acquisition
219 should be as efficient as possible. In laboratory conditions, this usually means that large flat-panel
220 detectors with thick scintillators need to be used. In recent years, the highest achievable frame rate of
221 these systems has drastically increased to values ranging from several tens of frames per second for full-
222 frame acquisition to several hundreds of frames per second for limited region readout, while several
223 experimental detector systems perform even better [27,28]. At the same time, the increased availability of
224 large amounts of fast computer memory allowed for the implementation of fast acquisition schemes, no
225 longer limited by the processing speed of hard drives. These two developments have drastically increased
226 the possibilities of fast and continuous CT scanning. When even higher scanning rates are needed, high-
227 speed line detector systems are to be used. However, they can scan only one or several lines at a time,
228 drastically limiting the field-of-view and therefore the ability of these setups to create 3D images. For
229 both detector types however, the temporal behavior of scintillators may in some cases become an issue at
230 high frame rates (i.e. cause detector lag).

231 As an alternative to flat-panel detectors with scintillators, direct or hybrid detector systems have been
232 developed over the last few years. These detector systems have no scintillator screen, but convert the
233 absorbed X-rays directly into electron-hole pairs. This detection method increases the response speed, and
234 allows for energy discriminating possibilities based on pulse height analysis. The latter allows for energy-

235 dispersive acquisition and for a drastic reduction of electronic noise. These systems have been reported to
236 have frame rates in the kHz range [29,30]. These very high frame rate detectors are primarily developed
237 for synchrotron applications [31,32] such as ptychographic imaging [33]. Consequently, they often use Si
238 as detecting material, given the low X-ray energy typically used in coherent diffractive imaging. Using
239 materials such as CdTe, which have a larger efficiency at high X-ray energies [34], the further
240 developments of photon counting detectors may in the near future also benefit laboratory-based dynamic
241 CT scanning.

242 **2.1.3 Add-on equipment for sample conditioning**

243 To investigate how fluids migrate through pores in a rock or how the minerals in the rock react over time,
244 the geological sample needs to be subjected to controlled external conditions, e.g. mechanical loading
245 [35], temperature [36] or humidity, possibly combined with the injection of pressurized liquids or gasses
246 [37]. Specialized add-on equipment for the micro-CT setup is thus needed in order to visualize the sample
247 at the desired in-situ conditions. It is not the intended scope of this paper to give a comprehensive
248 overview of add-on equipment used for in-situ imaging applied in the literature, but rather to briefly
249 highlight the limitations and challenges brought forth by this equipment, more specifically by flow cells.
250 The main concerns related to such flow cell setups, especially for fast laboratory-based micro-CT
251 imaging, are the size of the setup and the materials out of which it is constructed. Lab-based micro-CT
252 commonly achieves geometrical magnification by using conical X-ray beams. This means that the
253 diameter of the flow cell should be small in order to achieve high magnifications and correspondingly
254 high resolutions (depending on the characteristics of the scanner) while simultaneously maximizing the
255 use of the available X-ray flux (i.e. without having to increase the focus-detector distance more than
256 necessary) [1,16]. This is crucial to discriminate the pore network in the sample with sufficient detail.
257 Furthermore, the parts of the cell which are in the field of view should attenuate the X-ray beam as little
258 as possible to maximize the X-ray flux. At low cell pressures, low-cost plastics (e.g. PMMA) and epoxies
259 [38,39] are suitable, as these have a low X-ray attenuation coefficient compared to most geological
260 materials. However, to simulate reservoir conditions, high pressures (typically 100 - 500 bar) and
261 temperatures (typically 50-200°C) are required. The steel alloys (e.g. hastelloy) which are typically used
262 to build Hassler cells for flow experiments at these conditions are highly attenuating and therefore not
263 suitable for X-ray micro-CT imaging. Instead, imaging experiments require miniature Hassler cells
264 constructed out of weakly attenuating, strong materials like aluminum [40], carbon-based materials [41–
265 43], beryllium [2], and special plastics like PEEK [37].

266 **2.2 SOFTWARE ADVANCES**

267 **2.2.1 Advances in reconstruction algorithms**

268 In addition to specific requirements for acquisition hardware to optimize 4D scanning, major
269 improvements can also be achieved by applying clever software algorithms, mainly in terms of
270 tomographic reconstruction. The main challenge posed by laboratory-based fast CT is Poisson noise,
271 induced by the limited X-ray flux. Additionally, structural changes of the scanned sample during a CT
272 acquisition will cause motion blurring artefacts which deteriorate the reconstruction quality. Methods to
273 cope with both motion blurring and bad image statistics are thus crucial in dealing with fast imaging of
274 dynamic processes.

275 Currently, most tomographic reconstructions are performed using analytical filtered back-projection
276 (FBP) methods, such as the Feldmann-Davis-Kress (FDK) algorithm [44,45]. These algorithms have the
277 advantage of being relatively simple and fast in terms of computational complexity, but theoretically they
278 are only valid in idealized cases (i.e. when enough projections are acquired). In the context of (dynamic)

279 CT imaging, iterative reconstruction techniques [46,47] have gained much interest. During iterative
280 reconstruction, intermediate solutions of the reconstructed 3D object are incrementally refined by
281 simulating projection images from this solution (by forward projection) and subsequently adapting it to
282 better reproduce the experimental projections. Unlike analytical algorithms, the iterative techniques can
283 incorporate a priori knowledge about the measured object, drastically decreasing the degrees of freedom
284 in the reconstruction process. Furthermore, accurate models for specific physical and geometrical features
285 of the acquisition process can be modeled into the reconstruction, opening the possibility to include
286 corrections for imaging artifacts, e.g. beam hardening [48,49].

287 In general, a priori knowledge in CT leverages the spatial and temporal correlations which exists between
288 neighboring voxels in a volume throughout time. It can be implemented in several ways, e.g. by assuming
289 the scanned object is only made up of a limited number of clearly separated materials, corresponding to
290 an equally limited number of discrete gray values. This is typically done by a segmentation of the
291 intermediate result before a forward projection is performed. In doing so, the final result can typically be
292 obtained using fewer projection images, and no longer contains image noise. Furthermore, as image
293 segmentation is in most cases the first step in 3D analysis, these reconstruction methods have the
294 capability to make this processing step obsolete. Several reconstruction algorithms for this so-called
295 *discrete tomography* have been developed in recent years [50–52]. They differ mainly in the segmentation
296 method, in the moment of the appearance of the segmentation in the flow of the algorithm, and in
297 additional strategies to reduce noise effects in the segmentation of (partially) reconstructed volumes.

298 Another way of using prior knowledge is to incorporate information about the object's shape. The
299 simplest approach is to provide an appropriate initial intermediate solution to the iterative reconstruction
300 method. The drawback of this method is that this initial solution can become too dominant, obscuring
301 details which are actually changing in time. Other, more advanced methods indirectly incorporate the
302 initial solution by reconstructing the difference between the initial volume and the temporally changing
303 volume, as in prior image constrained compressed sensing (PICCS) [53,54]. Indeed, the difference
304 between these volumes will primarily highlight the regions of the volume which are structurally changing
305 through time. One of the more accomplished iterative reconstruction method for dynamic porous media
306 applications so far has been developed at ANU, and combines the notion of compressed sensing (cfr.
307 PICCS) with discrete tomography [15,55,56]. The method has been used for two-phase flow experiments
308 and formulates the reconstruction as an optimization problem over all discrete two-grey level solutions
309 which honor the static pore structure, while accommodating for the expected physical two-phase flow
310 behavior by adding extra regularization terms to the optimization cost function.

311 The dynamically evolving regions can also be estimated directly from the dynamic CT data itself, i.e.
312 without introducing an initial solution [57]. Finally, temporal correlations can be exploited by modeling
313 the expected deformation of the object as a function of time [58]. However, computational feasibility
314 limits the number of parameters, which restricts the deformation models to fairly global ones, affecting
315 the object as a whole, e.g. affine deformations.

316 It should be clear that aforementioned methods are only valid within specific constraints. Discrete
317 reconstruction methods are not applicable for complex multi-material objects where partial volume effects
318 are important. They are however very well suited for the imaging of homogeneous structures which are
319 changing in time, e.g. foams under compression. Methods applying initial solutions on the other hand are
320 well suited for the imaging of rigid structures in which small regions are changing in time, e.g. fluid flow
321 through a geological sample. Vast, non-local, structural changes however are more difficult to correct for
322 with these methods, in this case the reconstruction methods based on deformation models are more
323 suitable.

324 Next to alterations in the reconstruction step, some methods also rely on image pre-processing, by altering
 325 the projection. This is quite often the case for noise reduction methods or phase retrieval algorithms, some
 326 of which inherently include noise reduction. In filtered back-projection methods, the filter may also be
 327 adapted in order to reduce noise (typically at the expense of image sharpness).

328 **2.2.2 4D image analysis**

329 As the signal-to-noise ratio is of major concern in lab-based fast micro-CT, it may prove very important
 330 to make use of the redundancy of information in the time sequence when analyzing the data. This way, it
 331 should be possible to improve the 3D analysis (e.g. [2,59–61]) at one fixed time point by incorporating
 332 information from other time points. For example, 4D filtering methods may be useful to reduce motion
 333 artifacts and even to compensate for noisy data. To our knowledge, very little work on this topic has been
 334 done in the context of high-resolution CT research. However, we see a large potential for methods which
 335 have recently been developed for medical imaging purposes, e.g. 4D filters designed for CT perfusion
 336 scans [62–64] and for magnetic resonance imaging [65,66].

337 Another key principle to improve the quality of the analysis is the use of high quality scans performed at
 338 initial or final states of the sample. For example, one can segment the pore space from a prior high quality
 339 scan and use it as an analysis mask for the dynamic scans (as demonstrated in section 3 of this work).
 340 This rather simple approach is only applicable when the pore structure does not deform during the
 341 experiment and when the high-quality dataset can be spatially matched to the dynamic datasets (either by
 342 not moving the sample between acquisitions or by applying image registration algorithms, e.g. [67,68]).

343 Next to using redundant and prior information, 4D datasets call for algorithms to quantify a sample's
 344 evolution through time. In some cases it may be sufficient to perform 3D analysis on datasets of
 345 consecutive time steps and compare the results. It should be noted that in this case, it should be possible
 346 to script the process which may cause problems when user-defined input parameters need to be varied for
 347 each time step. In many cases, it is interesting to quantify changes through time by tracking movement or
 348 deformation of structures in the sample. Methods to do this are often inspired by 2D digital image
 349 correlation, and referred to as digital volume correlation. However, this problem is not specific to
 350 laboratory-based micro-CT as it is of interest in synchrotron-based and medical CT as well. For this
 351 reason, it is not treated here and the interested reader is referred to [3,69–75].

352 **3 ILLUSTRATIVE APPLICATIONS**

353 **3.1 TWO-PHASE FLOW**

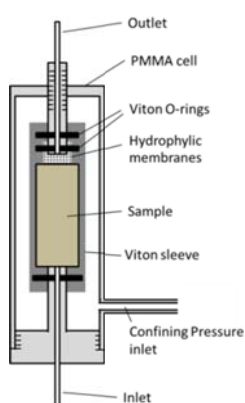
354 The flow of multiple fluid phases in porous rocks is essential to several important geo-engineering
 355 challenges, e.g. environmental remediation of aquifers polluted with non-aqueous phase liquids (NAPL),
 356 hydrocarbon recovery and CO₂-sequestration in geological reservoirs. The field-scale properties of these
 357 processes are critically determined by pore-scale fluid-fluid and fluid-solid interactions. In this section,
 358 we present an experiment where drainage of a Bentheimer sandstone was visualized under dynamic
 359 conditions (i.e. while continuously injecting non-wetting fluid) on a laboratory-based micro-CT scanner at
 360 Ghent University's Centre for X-ray Tomography (UGCT). We show the observation of pore filling
 361 events which bear strong resemblance to Haines jumps, even though we did not record pressure
 362 measurements at the time of the experiment to prove this. To our knowledge, it is the first time
 363 observations of this kind have been made on a laboratory-based micro-CT system.

364 While a detailed explanation of the physics of drainage is out of the scope of this article, we outline the
 365 motivation to perform this experiment. During drainage, the displacement process happens by fast,

366 irreversible events (Haines jumps) alternated by smooth, reversible displacement related to fluid storage
367 in pinned interfaces [76,77]. Such a Haines jump corresponds to the filling of a single geometrical pore
368 body. These jumps frequently happen in cascades, classically explained as successive filling of pores with
369 lower entry capillary pressure than the first pore of the cascade. The rate of non-wetting fluid injection
370 does not influence the duration of individual Haines jumps, but it does influence their frequency. Single
371 pore events have been found to transpire on the millisecond time scale [76], and [77] states that cascades
372 of pore filling events take place on a time scale of typically 0.5 to 2 seconds. Clearly, to investigate
373 dynamic effects related to the irreversible displacement, it is crucial not to interrupt the non-wetting fluid
374 injection during the imaging. In their groundbreaking work on real-time visualization of two-phase flow
375 in natural stone, executed at the TOMCAT beamline of the Swiss Light Source synchrotron facility, Berg
376 et al. [6] were able to perform such an experiment for the first time. In this study, they suggest that
377 dynamic effects cause pore filling events to be non-local. Since then, this topic has been investigated
378 further [77,78], yet many aspects of the occurring dynamic effects and particularly of their influence on
379 larger-scale petrophysical properties remain unclear. Further imaging experiments may thus prove
380 extremely valuable in understanding these processes.

381 **3.1.1 Materials and methods**

382 In this experiment, the sample was a German Bentheimer sandstone of the Gildehaus variety from the
383 Early-Cretaceous. Its rather homogeneous pore size distribution render it ideally suited for micro-CT
384 studies. A sample with a diameter of 6 mm and a height of 17 mm was put in a Viton sleeve and set into a
385 custom-built, low-cost PMMA flow cell (Figure 2). The flowcell was mounted on UGCT's
386 Environmental Micro-CT scanner (EMCT, Figure 2), designed and built in-house in collaboration with X-
387 Ray Engineering bvba (XRE, Ghent, Belgium). This scanner is specially developed to image samples
388 under controlled environmental conditions or during dynamic experiments. To allow for the sample and
389 the equipment connected to it with wires or tubing to remain static, the setup has a rotating X-ray source
390 and detector assembly on a gantry. This eliminates problems with flow instabilities caused by bending or
391 twisting of the flow lines, and it helps avoid unwanted sample movement during the acquisition.
392 Unlimited continuous rotation is possible because electrical power and safety interlocks are transmitted
393 through slip-rings. The system is equipped with a standard directional microfocus X-ray tube with
394 integrated high-voltage power supply (maximum high voltage 130 kV, maximum power output 39 W,
395 minimum spot size 5 μ m). The detector is a CMOS flat-panel detector (1316 by 1312 pixels with a 100
396 μ m pitch) with a thick, structured CsI scintillator. The GigE-interface permits frame rates of 30 fps at full
397 resolution and 60 fps in 2x2 binned mode (and even more in panoramic mode). The scanner's source-
398 detector combination, together with the applied smooth-scanning (rather than step-and-shoot) acquisition,
399 allows for fast scanning. More details on EMCT's setup can be found in [79], although the rotation motor
400 has since been upgraded to allow for faster scanning.



401

402 **Figure 2.** A custom-built PMMA confining-pressure flowcell (left) allows the visualization of fluid flow
 403 in stone samples with a diameter of 6 mm and a height between 15 and 20 mm. UGCT's EMCT scanner
 404 (right) was built in collaboration with XRE. The flow cell is mounted on a stand which moves into the
 405 scanner from below. The gantry (with the source and detector mounted on it) rotates around the sample,
 406 while the sample remains static.

407 The sample was first saturated with water by flushing with CO₂ and subsequently with water. At this
 408 point, a first high-quality scan (Table 1) of the sample was performed to obtain geometric information of
 409 the sample's pore space. Then, a highly X-ray-attenuating brine (10 wt% CsCl) was pumped through the
 410 sample. A second high-quality scan confirmed that the sample was completely brine-saturated.
 411 Subsequently, drainage was started by pumping an oil phase (kerosene or 'paraffin') into the sample at a
 412 flow rate of 6 μl/min. This corresponds to a capillary number [80] of approximately $7 \cdot 10^{-8}$, a realistic
 413 value for real reservoir flow processes. Fast scans were performed with settings outlined in Table 1.
 414 Projections were continuously acquired during a 5 minute time interval, during which the drainage was
 415 not halted (except near the beginning and end of the acquisition).

416 The fast scans were recorded and processed with the proprietary 4D tools of the ACQUILA software
 417 (XRE, Ghent, Belgium). Because the acquisition is continuous, projections acquired during any full
 418 rotation of the gantry can be reconstructed regardless of the starting angle. In this experiment, we
 419 generated a new reconstruction after every 120° rotation of the gantry, meaning consecutive
 420 reconstructions in the time series are 4 seconds apart. This results in a total of 72 reconstructions in the 5
 421 minute acquisition. Tomographic reconstruction was performed with the FDK algorithm, implemented on
 422 the GPU.

423 **Table 1.** Settings of scans performed in the drainage experiments

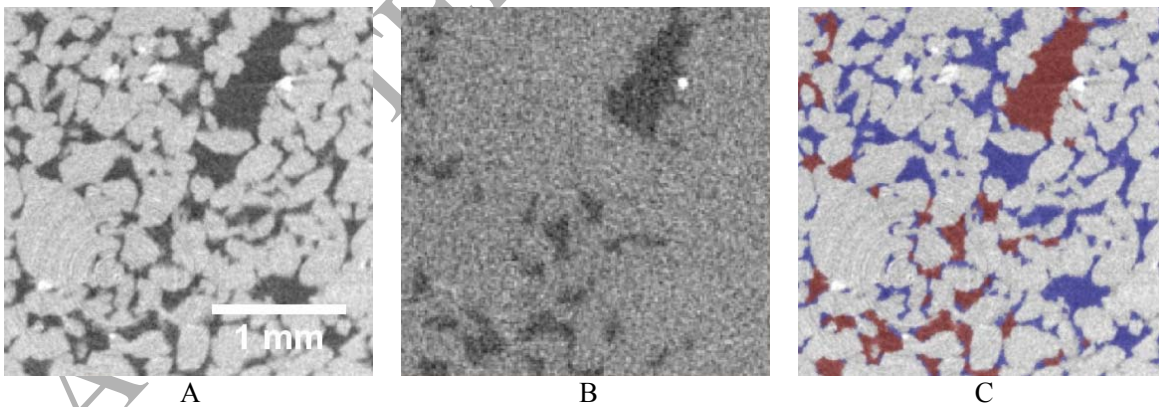
	High quality	Fast scans
Voxel size (μm)	7.4	14.8
Total time per scan	21 min	12 s
Binning of detector pixels	No	Yes (2x2)
Amount of voxels/scan	1314x1314x1311	657x657x656
Projection exposure time (ms)	550	20
Projections per 360° scan	2200	600
Accelerating voltage (kV)	80	130
X-ray source output (W)	8	16
Source-detector distance (mm)		365.0
Source-object distance (mm)		27.1

424

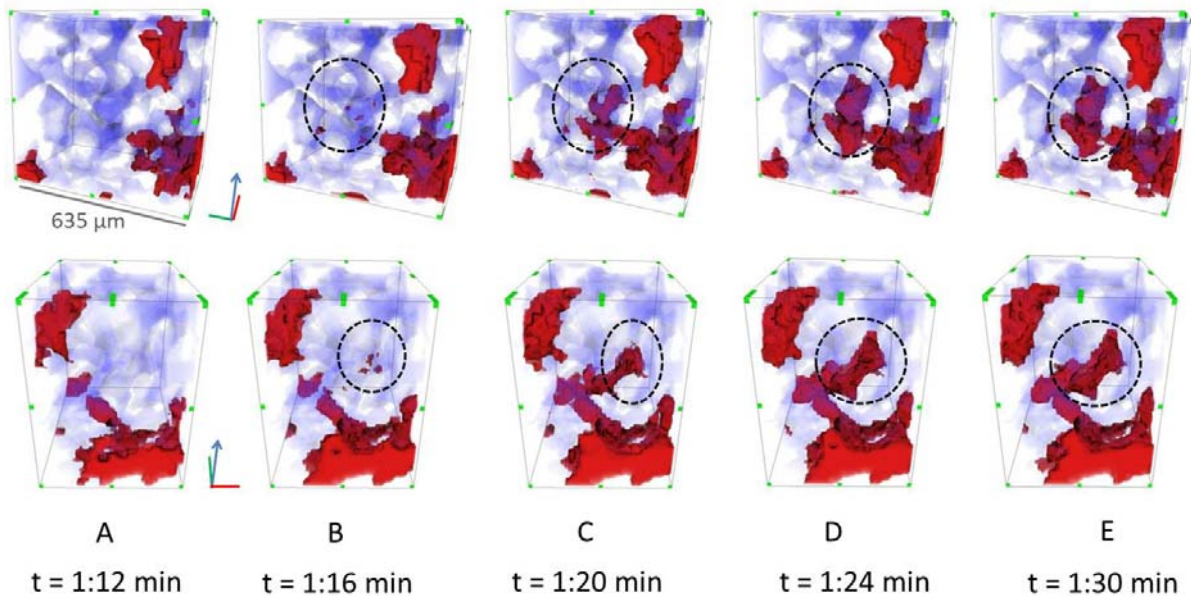
425 **3.1.2 Results and discussion**

426 The high-quality scan of the pore space (filled with pure water) was segmented to identify pore and solid
 427 voxels. The fast scans were first treated with an anisotropic diffusion filter in Avizo (VSG/FEI, France)
 428 and then resampled without interpolation with a factor two to contain as many voxels as the high-quality
 429 scan. The oil phase was subsequently segmented from each fast scan, with the pore space identified from
 430 the high-quality scan applied as a mask. This way, prior information on the pore space geometry was
 431 incorporated post-reconstruction. This information can also be used during reconstruction, if some
 432 assumptions on the transpiring pore-scale process are made [14]. Using this approach, Myers and
 433 coworkers [14,15] reported lab-based scans of two-phase flow under dynamic conditions, at 85 seconds
 434 per scan with a voxel size of 12 μm .

435 After recombining the oil segmentations with the pore space segmentation, 3-phase segmentations (oil,
 436 water and solid) were obtained for each timestep. Example slices showing the segmentation quality can be
 437 seen in Figure 3 (additionally, example slices can be found in supplementary materials). While it is clear
 438 that the resolution of the scans is insufficient to detect the oil-phase in some of the smallest pores, the fast
 439 scans evidently contain much information on the rock's drainage behavior and allow pore filling events
 440 like the one circled in Figure 4 to be investigated. By comparison with results shown in [6], this figure is
 441 likely to show an individual Haines jump (note that the apparently gradual filling of the pore is due to
 442 remaining motion artifacts in the reconstruction). Further analysis of the experiment is presented in [81].
 443 It can be concluded that it is becoming possible to visualize the fundamental pore-scale processes which
 444 govern drainage in geological porous media with laboratory-based micro-CT scanners, despite remaining
 445 challenges related to spatial and time resolution. With regard to the former challenge, it should be noted
 446 that the rather simple flow cell used in this work could be designed more efficiently. This way, it may be
 447 possible to minimize X-ray absorption by the cell and to reduce the source-to-sample distance, resulting
 448 in larger magnifications. With regard to the latter, selecting a set of projections representing a 360°
 449 rotation can be done more efficiently by detecting pore-scale events on the radiographs, in a similar way
 450 as shown by [8]. This method results in the elimination of motion artifacts for selected events.



451 **Figure 3.** This figure suggests that the image quality is sufficient to visualize most oil-filled pores (with
 452 the exception of oil in very fine pore space features). Figure A shows a cropped slice from the high-
 453 quality scan (7.4 μm voxel size). By applying the pore space mask determined from A and segmenting the
 454 fast scan (12 s) in B, the pore space voxels were segmented into the oil phase (red) and the brine phase
 455 (blue) (C). Figure B was recorded after 4 minutes of running the drainage experiment (60th scan in the
 456 time series). Note that due to the highly-attenuating CsCl, the brine could not be distinguished from the
 457 stone in the fast scans.



458

459 **Figure 4.** This time sequence shows a pore filling event (circled) during drainage from two viewing
 460 angles. The non-wetting phase is visualized in red, the wetting phase in transparent blue. The reported
 461 time is the starting time of the micro-CT acquisition. Each acquisition took 12 seconds.

462 3.2 SOLUTE TRANSPORT

463 In this section, we describe an experiment aimed at elucidating solute transport in heterogeneous rocks. In
 464 groundwater systems, mixing of reactants often limits (bio)chemical reactions [82]. In CO₂ sequestration
 465 and enhanced oil recovery, CO₂ dissolved in brine can trigger dissolution and precipitation of minerals in
 466 the host rock's pore space, in turn affecting this rock's mechanical and fluid flow properties [43]. The
 467 transport phenomena and simultaneous chemical reactions in these processes are coupled, and one can
 468 therefore only begin to understand the dissolution and precipitation patterns and the resulting flow
 469 properties, if one also understands solute transport by advection and diffusion in the pore space. In
 470 heterogeneous media, particularly carbonates, the pore-level flow field can show significant channeling
 471 [83]. This implies that important differences in fluid chemistry can arise between the more stagnant
 472 regions and the channels with a higher advective transport rate, which in turn will influence the
 473 dissolution behavior in the carbonate host rock. Depending on the balance between advection, diffusion
 474 and reaction rates, the dissolution reaction can cause the preferential flow channels to become
 475 increasingly wide. This behavior is often referred to as wormholing [84], and can have important field-
 476 scale consequences (e.g. [85]).

477 We show the feasibility of imaging solute transport (diffusion and advection) in 3D in a carbonate at the
 478 pore scale. While some studies have investigated the imaging of solute transport [86–89], to our
 479 knowledge this has not been undertaken before simultaneously at the pore scale and at the time scale (12
 480 seconds per scan) shown here. While the discussion will be restricted to one experiment (a single imposed
 481 flow rate), by varying the flow rate a detailed study of pore scale dispersion can be undertaken. Such
 482 studies may prove vital as a validation to solute transport modeling methods described in for example
 483 [90,91] and as input to characterize the connectivity of microporosity in multi-scale modeling [92,93].

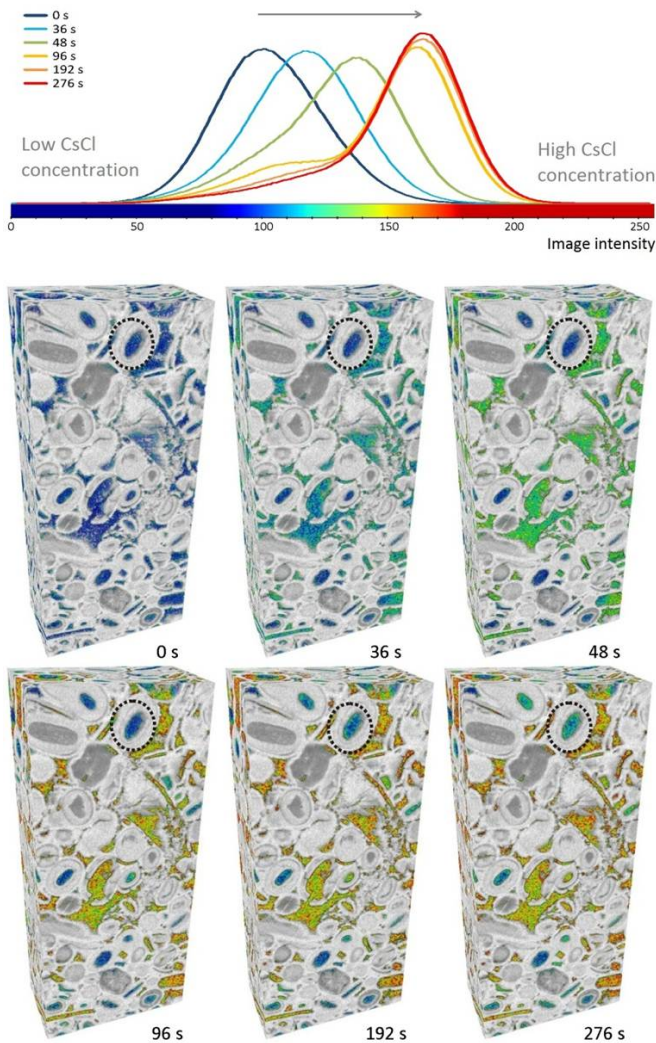
484 3.2.1 Materials and methods

485 In the experiment outlined here, transport of a tracer salt subject to diffusion and advection is investigated
486 in the Savonnières limestone, a French oolitic limestone (Late Jurassic). This grain-supported limestone
487 consists of ooids and shell fragments bound together by sparite. During diagenesis, some of these grain
488 fragments were partially dissolved resulting in a pore network with well-connected pores between the
489 grains (intergranular porosity) and secondary porosity inside the dissolved grains (intragranular porosity
490 or vuggy porosity), which is connected to the rest of the pore network through microporosity [94].
491 Preferential flow channels were visualized by pumping a highly X-ray attenuating brine (containing 10
492 wt% CsCl) into a water-saturated sample at a flow rate of 0.6 ml/min. The sample had a diameter of 6 mm
493 and was placed in the PMMA flow cell (Figure 2). Fast laboratory-based micro-CT scans were performed
494 with EMCT (12 seconds/scan). Scan parameters were the same as the fast scans described in section
495 3.1.1. Similarly to the workflow described in that section, a high-quality scan was used to segment a mask
496 for the macropores.

497 3.2.2 Results and discussion

498 In Figure 5, the histogram of the reconstructed image intensity values inside the macropore voxels
499 (selected by applying the pore space mask) in the limestone is given for the different timesteps. The peak
500 at 0 seconds shows the distribution of the intensity values before brine injection. At this stage, all voxels
501 included in the histogram (i.e. all voxels in the macro-pore space) are filled with pure water. This is also
502 illustrated in the rendering in this figure, where at 0 seconds the image intensity values in the pore space
503 are low and homogeneously distributed. During injection, the histogram shifts to the right and after 96
504 seconds, the intensity values are distributed in two peaks. This indicates a heterogeneous distribution of
505 the CsCl concentration in the pore space of the limestone sample. The renderings show that most of the
506 intergranular pore space contains a high CsCl concentration, while the intragranular pores in the dissolved
507 ooids (Figure 5, dotted circle) still have a low CsCl concentration. In later timesteps, the peak on the left
508 side of the histogram starts to disappear. This corresponds to the gradual increase of the CsCl
509 concentration in the intragranular pores, which can be seen in the renderings. After a long waiting time,
510 the histogram of the pore space voxels will again consist of one single peak, but centered around a higher
511 average grey value than in the initial condition.

512 The results illustrate that the distribution of the brine in the intergranular pore space is mainly controlled
513 by advection. In these pores, preferential flow paths can be found. The flow in the intragranular pores is
514 more stagnant and the concentration of CsCl in this vuggy pore space is therefore mainly controlled by
515 diffusion. Fitting with the scope of this article, more elaborate analysis of the data will be presented
516 elsewhere. Although the measurements presented here are clearly a good indication of CsCl-
517 concentrations in the sample, further research will be performed to calibrate the image intensity values to
518 exact concentration values.



519

520 **Figure 5.** The graphs show the evolution of the image intensity histograms of (only) the pore space
 521 voxels in the Savonnières limestone sample during brine injection. High image intensities correspond to
 522 high CsCl-concentrations. The corresponding 3D rendering show the evolution of the CsCl concentration
 523 in the macropores. The dotted circle indicates an intragranular pore in which the flow is stagnant. Time
 524 series measurements were performed with the EMCT-scanner at an acquisition time of 12 seconds.

525

526 4 CONCLUSIONS

527 Micro-CT scanning with a sub-minute time resolution is a very desirable experimental technique, both as
 528 an accessible stand-alone tool to investigate dynamic pore-scale processes and to prepare experiments for
 529 much more restricted yet higher-quality synchrotron measurements. A number of difficulties, mainly
 530 related to the limited X-ray flux, have hampered the implementation of such set-ups. Future developments
 531 in X-ray source and detector technology (notably the improvement and implementation of liquid-metal jet
 532 sources and photon-counting detectors) may increase the attainable time resolution and improve the
 533 image quality and spatial resolution at short acquisition time. We also expect a significant contribution

534 from advanced tomographic iterative reconstruction and 4D image analysis algorithms, which can
535 compensate for the often limited image quality in fast scans by incorporating prior information about the
536 pore structure or the physical processes transpiring in the pore space. Furthermore, progress is being made
537 in automating 4D image processing and image analysis, making it more and more feasible to work with
538 large, computationally intensive time-series datasets.

539 Despite the limitations, we illustrate the large potential of fast micro-CT scanning with two cutting-edge
540 real-time imaging experiments. We show that it is possible to visualize single and few-pore drainage
541 events in a Bentheimer sandstone by continuously scanning the sample with UGCT's Environmental
542 Micro-CT (EMCT) scanner at an acquisition time of 12 seconds per full rotation. The same set-up and
543 settings were used to visualize pore scale solute transport of a tracer salt (CsCl) in a Savonnières
544 limestone, allowing to study the location of stagnant and fast flow regions and the relative time scales of
545 diffusion and advection in this stone.

546 As illustrated by these experiments, it is today becoming possible to study transport processes in
547 geological samples at the pore scale in a laboratory-setting, without having to impose quasi-static
548 conditions. We expect that with further improvements in image quality, real-time imaging with
549 laboratory-based micro-CT scanners will be implemented much more widely. This would provide
550 valuable feed-back to the pore scale modeling community and has the potential to strongly increase our
551 understanding of porous media behavior. In the long term, this may be beneficial to the management of
552 geological reservoirs and aquifers, as well as to a wide variety of other issues involving porous materials
553 (e.g. building stone deterioration, development of batteries and fuel cells, food engineering, textile
554 engineering).

555 ACKNOWLEDGEMENTS

556 We thank Dr. Rémi Blanc (FEI) for his assistance with handling 4D datasets in Avizo. Ioannis Zarikos is
557 acknowledged for helping to build and test the flow set-up (shown in section 3) during his master's thesis.
558 Dr. Hannelore Derluyn is thanked for helpful discussions. The Agency for Promotion of Innovation by
559 Science and Technology in Flanders, Belgium (IWT) is acknowledged for the PhD grant of Tom
560 Bultreys. The UGent Special Research Fund (BOF) is acknowledged for the post-doctoral grant of M.N.
561 Boone. This work was also partially supported by FWO, project G024212N and G.0041.15N.

562 BIBLIOGRAPHY

- 563 [1] Cnudde V, Boone MN. High-resolution X-ray computed tomography in geosciences: A review of
564 the current technology and applications. *Earth-Science Rev* 2013;123:1–17.
565 doi:http://dx.doi.org/10.1016/j.earscirev.2013.04.003.
- 566 [2] Wildenschild D, Sheppard AP. X-ray imaging and analysis techniques for quantifying pore-scale
567 structure and processes in subsurface porous medium systems. *Adv Water Resour* 2013;51:217–
568 46. doi:http://dx.doi.org/10.1016/j.advwatres.2012.07.018.
- 569 [3] Maire E, Withers PJ. Quantitative X-ray tomography. *Int Mater Rev* 2014;59:1–43.
570 doi:10.1179/1743280413Y.0000000023.

- 571 [4] Mokso R, Marone F, Haberthür D, Schittny JC, Mikuljan G, Isenegger A, et al. Following
572 Dynamic Processes by X-ray Tomographic Microscopy with Sub-second Temporal Resolution,
573 2011, p. 38–41. doi:10.1063/1.3625299.
- 574 [5] Rack A, Garcia-Moreno F, Schmitt C, Betz O, Cecilia A, Ershov A, et al. On the possibilities of
575 hard X-ray imaging with high spatio-temporal resolution using polychromatic synchrotron
576 radiation. *J Xray Sci Technol* 2010;18:429–41. doi:10.3233/XST-2010-0273.
- 577 [6] Berg S, Ott H, Klapp SA, Schwing A, Neiteler R, Brussee N, et al. Real-time 3D imaging of
578 Haines jumps in porous media flow. *Proc Natl Acad Sci* 2013;110:3755–9.
579 doi:10.1073/pnas.1221373110.
- 580 [7] Youssef S, Deschamps H, Dautriat J, Rosenberg E, Oughanem R, Maire E, et al. 4D Imaging of
581 fluid flow dynamics in natural porous media with ultra-fast X-ray microtomography. *Int. Symp.*
582 *Soc. Core Anal., Napa Valley, USA: Society of Core Analysts; 2013.*
- 583 [8] Armstrong RT, Georgiadis A, Ott H, Klemin D, Berg S. Critical capillary number: Desaturation
584 studied with fast X-ray computed microtomography. *Geophys Res Lett* 2014;41:55–60.
585 doi:10.1002/2013GL058075.
- 586 [9] Hoogland, F., P. Lehmann, F. Moebius, P. Vontobel DO. Liquid redistribution behind a drainage
587 front in porous media imaged by neutron radiography. *EGU Gen. Assem. Geophys. Res. Abstr.*,
588 Vienna, Austria: EGU; 2013, p. EGU2013–8156.
- 589 [10] Menke H, Bijeljic B, Andrew M, Blunt MJ. Dynamic Pore-scale Imaging of Reactive Transport in
590 Heterogeneous Carbonates at Reservoir Conditions. *Energy Procedia* 2014;63:5503–11.
591 doi:10.1016/j.egypro.2014.11.583.
- 592 [11] Baker DR, Brun F, O’Shaughnessy C, Mancini L, Fife JL, Rivers M. A four-dimensional X-ray
593 tomographic microscopy study of bubble growth in basaltic foam. *Nat Commun* 2012;3:1135.
594 doi:10.1038/ncomms2134.
- 595 [12] Eller J, Roth J, Marone F, Stampanoni M, Wokaun A, Büchi FN. Towards Ultra-Fast X-ray
596 Tomographic Microscopy of Liquid Water in PEFC. *ECS Trans* 2011;41:387–94.
597 doi:10.1149/1.3635572.
- 598 [13] Sedighi Gilani M, Fife JL, Boone MN, Ghazi Wakili K. Dynamics of microcrack propagation in
599 hardwood during heat treatment investigated by synchrotron-based X-ray tomographic
600 microscopy. *Wood Sci Technol* 2013;47:889–96. doi:10.1007/s00226-013-0545-8.
- 601 [14] Myers GR, Kingston AM, Varslot TK, Turner ML, Sheppard AP. Dynamic tomography with a
602 priori information. *Appl Opt* 2011;50:3685–90. doi:10.1364/AO.50.003685.
- 603 [15] GR Myers, AM Kingston, TK Varslot, ML Turner AS. Dynamic X-ray micro-tomography for real
604 time imaging of drainage and imbibition processes at the pore scale. *Int. Symp. Soc. Core Anal.*,
605 Society of Core Analysts; 2011.
- 606 [16] Sheppard A, Latham S, Middleton J, Kingston A, Myers G, Varslot T, et al. Techniques in helical
607 scanning, dynamic imaging and image segmentation for improved quantitative analysis with X-ray

- 608 micro-CT. Nucl Instruments Methods Phys Res Sect B Beam Interact with Mater Atoms
609 2014;324:49–56. doi:10.1016/j.nimb.2013.08.072.
- 610 [17] King A, Reischig P, Adrien J, Ludwig W. First laboratory X-ray diffraction contrast tomography
611 for grain mapping of polycrystals. J Appl Crystallogr 2013;46:1734–40.
612 doi:10.1107/S0021889813022553.
- 613 [18] Kaminski R, Nottingham G, Coppens P. An optical chopper for generation of short X-ray pulses to
614 allow in-house time-resolved photocrystallography. J Appl Crystallogr 2014;47:1765–8.
615 doi:10.1107/S160057671401961X.
- 616 [19] Larsson DH, Lundström U, Westermark UK, Arsenian Henriksson M, Burvall A, Hertz HM. First
617 application of liquid-metal-jet sources for small-animal imaging: high-resolution CT and phase-
618 contrast tumor demarcation. Med Phys 2013;40:021909. doi:10.1118/1.4788661.
- 619 [20] Zhou T, Lundström U, Thüring T. Comparison of two x-ray phase-contrast imaging methods with
620 a microfocus source. Opt Express 2013;21:1141–8. doi:10.1364/OE.21.030183.
- 621 [21] Lundström U, Larsson DH, Burvall A, Scott L, Westermark UK, Wilhelm M, et al. angiography
622 for sub-10 μm vessel imaging. Phys Med Biol 2012;57:7431–41. doi:10.1088/0031-
623 9155/57/22/7431.
- 624 [22] Bartels M, Hernandez VH, Krenkel M, Moser T, Salditt T. Phase contrast tomography of the
625 mouse cochlea at microfocus x-ray sources. Appl Phys Lett 2013;103. doi:10.1063/1.4818737.
- 626 [23] Espes E, Andersson T, Björnsson F, Gratorp C, Hansson BAM, Hemberg O, et al. Liquid-metal-jet
627 x-ray tube technology and tomography applications. SPIE Opt. Eng. + Appl., International Society
628 for Optics and Photonics; 2014, p. 92120J. doi:10.1117/12.2061612.
- 629 [24] Larsson DH, Takman PAC, Lundström U, Burvall A, Hertz HM. A 24 keV liquid-metal-jet x-ray
630 source for biomedical applications. Rev Sci Instrum 2011;82. doi:10.1063/1.3664870.
- 631 [25] Ettl E, Schleede S, Bech M, Achterhold K, Loewen R, Ruth RD, et al. X-ray phase-contrast
632 tomography with a compact laser-driven synchrotron source. Proc Natl Acad Sci
633 2015;112:201500938. doi:10.1073/pnas.1500938112.
- 634 [26] Graves WS, Bessuille J, Brown P, Carbajo S, Dolgashev V, Hong K-H, et al. Compact x-ray
635 source based on burst-mode inverse Compton scattering at 100 kHz. Phys Rev Spec Top - Accel
636 Beams 2014;17. doi:10.1103/PhysRevSTAB.17.120701.
- 637 [27] Krymski AI, Bock NE, Tu N, Van Blerkom D, Fossum ER. A high-speed, 240-frames/s, 4.1-
638 Mpixel CMOS sensor. IEEE Trans Electron Devices 2003;50:130–5.
639 doi:10.1109/TED.2002.806961.
- 640 [28] Singh B, Miller SR, Bhandari HB, Graceffa R, Irving TC, Nagarkar V V. High-speed detector for
641 time-resolved diffraction studies. J Phys Conf Ser 2013;425. doi:10.1088/1742-
642 6596/425/9/092005.

- 643 [29] Szczygiel R, Grybos P, Maj P. High frame rate measurements of semiconductor pixel detector
644 readout IC. *Nucl Instruments Methods Phys Res Sect A Accel Spectrometers, Detect Assoc Equip*
645 2012;680:56–60. doi:10.1016/j.nima.2012.03.045.
- 646 [30] Dinapoli R, Bergamaschi A, Henrich B, Horisberger R, Johnson I, Kraft P, et al. A new family of
647 pixel detectors for high frame rate X-ray applications. *Nucl. Instruments Methods Phys. Res. Sect.*
648 *A Accel. Spectrometers, Detect. Assoc. Equip.*, vol. 617, 2010, p. 384–6.
649 doi:10.1016/j.nima.2009.10.043.
- 650 [31] Johnson I, Bergamaschi A, Billich H, Cartier S, Dinapoli R, Greiffenberg D, et al. Eiger: a single-
651 photon counting x-ray detector. *J Instrum* 2014;9. doi:10.1088/1748-0221/9/05/C05032.
- 652 [32] Henrich B, Bergamaschi A, Broennimann C, Dinapoli R, Eikenberry EF, Johnson I, et al.
653 PILATUS: A single photon counting pixel detector for X-ray applications. *Nucl Instruments*
654 *Methods Phys Res Sect A Accel Spectrometers, Detect Assoc Equip* 2009;607:247–9.
655 doi:10.1016/j.nima.2009.03.200.
- 656 [33] Guizar-Sicairos M, Johnson I, Diaz A, Holler M, Karvinen P, Stadler H-C, et al. High-throughput
657 ptychography using eiger: scanning x-ray nano-imaging of extended regions. *Opt Express*
658 2014;22:14859–70.
- 659 [34] Koenig T, Schulze J, Zuber M, Rink K, Butzer J, Hamann E, et al. Imaging properties of small-
660 pixel spectroscopic x-ray detectors based on cadmium telluride sensors. *Phys Med Biol*
661 2012;57:6743–59. doi:10.1088/0031-9155/57/21/6743.
- 662 [35] Bale H a, Haboub A, MacDowell A a, Nasiatka JR, Parkinson DY, Cox BN, et al. Real-time
663 quantitative imaging of failure events in materials under load at temperatures above 1,600 °C. *Nat*
664 *Mater* 2013;12:40–6. doi:10.1038/nmat3497.
- 665 [36] De Kock T, Boone M, Dewanckele J, Boever W De, Boone M, Schutter G De, et al. Monitoring
666 frost susceptibility of limestone faces. *12th Int. Congr. Deterior. Conserv. Stone*, vol. 1889, 2013.
- 667 [37] Boone MA, Nielsen P, De Kock T, Boone MN, Quaghebeur M, Cnudde V. Monitoring of
668 stainless-steel slag carbonation using X-ray computed microtomography. *Environ Sci Technol*
669 2014;48:674–80. doi:10.1021/es402767q.
- 670 [38] Pak T, Butler I, van Dijke MIJ, Geiger S, Jiang Z. Visualisation of Two-Phase Fluid Displacement
671 Processes at Pore Scale in Carbonate Rocks using Computed Tomography Technique.
672 *ICTMS2013*, 2013, p. 5–8.
- 673 [39] Herring AL, Harper EJ, Andersson L, Sheppard A, Bay BK, Wildenschild D. Effect of fluid
674 topology on residual nonwetting phase trapping: Implications for geologic CO₂ sequestration. *Adv*
675 *Water Resour* 2013;62:47–58. doi:10.1016/j.advwatres.2013.09.015.
- 676 [40] Fuisseis F, Steeb H, Xiao X, Zhu W, Butler IB, Elphick S, et al. A low-cost X-ray-transparent
677 experimental cell for synchrotron-based X-ray microtomography studies under geological
678 reservoir conditions. *J Synchrotron Radiat* 2014;21:251–3. doi:10.1107/S1600577513026969.

- 679 [41] Iglauer S, Paluszny A, Pentland CH, Blunt MJ. Residual CO₂ imaged with X-ray micro-
680 tomography. *Geophys Res Lett* 2011;38:n/a – n/a. doi:10.1029/2011GL049680.
- 681 [42] Andrew M, Bijeljic B, Blunt MJ. Pore-scale imaging of trapped supercritical carbon dioxide in
682 sandstones and carbonates. *Int J Greenh Gas Control* 2014;22:1–14.
683 doi:10.1016/j.ijggc.2013.12.018.
- 684 [43] Ott H, de Kloe K, van Bakel M, Vos F, van Pelt A, Legerstee P, et al. Core-flood experiment for
685 transport of reactive fluids in rocks. *Rev Sci Instrum* 2012;83:084501. doi:10.1063/1.4746997.
- 686 [44] Kak AC, Slaney M. Principles of computerized tomographic imaging. IEEE Press; 1988.
- 687 [45] Feldkamp L a., Davis LC, Kress JW. Practical cone-beam algorithm. *J Opt Soc Am A* 1984;1:612.
688 doi:10.1364/JOSAA.1.000612.
- 689 [46] Herman GT, Lent A. Iterative reconstruction algorithms. *Comput Biol Med* 1976;6:273–94.
690 doi:10.1016/0010-4825(76)90066-4.
- 691 [47] Andersen AH, Kak AC. Simultaneous algebraic reconstruction technique (SART): a superior
692 implementation of the art algorithm. *Ultrason Imaging* 1984;6:81–94. doi:10.1016/0161-
693 7346(84)90008-7.
- 694 [48] Brabant L, Pauwels E, Dierick M, Van Loo D, Boone MA, Van Hoorebeke L. A novel beam
695 hardening correction method requiring no prior knowledge, incorporated in an iterative
696 reconstruction algorithm. *NDT E Int* 2012;51:68–73. doi:10.1016/j.ndteint.2012.07.002.
- 697 [49] De Man B, Nuyts J, Dupont P, Marchal G, Suetens P. An iterative maximum-likelihood
698 polychromatic algorithm for CT. *IEEE Trans Med Imaging* 2001;20:999–1008.
699 doi:10.1109/42.959297.
- 700 [50] Brabant L, Dierick M, Pauwels E, Boone MN, Hoorebeke L Van. EDART, a discrete algebraic
701 reconstructing technique for experimental data obtained with high resolution computed
702 tomography. *J Xray Sci Technol* 2014;22:47–61. doi:10.3233/XST-130408.
- 703 [51] Herman GT, Kuba A. Advances in discrete tomography and its applications. Springer Science &
704 Business Media. Springer Science & Business Media; 2008.
- 705 [52] Batenburg KJ, Sijbers J. DART: A Practical Reconstruction Algorithm for Discrete Tomography.
706 *IEEE Trans Image Process* 2011;20:2542–53. doi:10.1109/TIP.2011.2131661.
- 707 [53] Chen G-H, Tang J, Leng S. Prior image constrained compressed sensing (PICCS): a method to
708 accurately reconstruct dynamic CT images from highly undersampled projection data sets. *Med*
709 *Phys* 2008;35:660–3. doi:10.1118/1.2836423.
- 710 [54] Lee J, Stayman JW, Otake Y, Schafer S, Zbijewski W, Khanna AJ, et al. Volume-of-change cone-
711 beam CT for image-guided surgery. *Phys Med Biol* 2012;57:4969–89. doi:10.1088/0031-
712 9155/57/15/4969.

- 713 [55] Myers GR, Kingston AM, Varslot TK, Turner ML, Sheppard AP. Dynamic tomography with a
714 priori information. *Appl Opt* 2011;50:3685–90. doi:10.1364/AO.50.003685.
- 715 [56] Myers G, Varslot T, Kingston A, Herring A, Sheppard AP. Ground-truth verification of dynamic
716 x-ray micro-tomography images of fluid displacement. vol. 8506, 2012, p. 85060P – 85060P – 7.
717 doi:10.1117/12.929410.
- 718 [57] Van Eyndhoven G, Batenburg KJ, Sijbers J. Region-based iterative reconstruction of structurally
719 changing objects in CT. *IEEE Trans Image Process* 2014;23:909–19.
720 doi:10.1109/TIP.2013.2297024.
- 721 [58] Mooser R, Forsberg F, Hack E, Székely G, Sennhauser U. Estimation of affine transformations
722 directly from tomographic projections in two and three dimensions. *Mach Vis Appl* 2013;24:419–
723 34. doi:10.1007/s00138-011-0376-2.
- 724 [59] Kaestner a., Lehmann E, Stampanoni M. Imaging and image processing in porous media research.
725 *Adv Water Resour* 2008;31:1174–87. doi:10.1016/j.advwatres.2008.01.022.
- 726 [60] Russ JC. *The Image Processing Handbook*. 4th ed. Boca Raton, FL: CRC Press; 2002.
- 727 [61] Brabant L, Vlassenbroeck J, De Witte Y, Cnudde V, Boone MN, Dewanckele J, et al. Three-
728 dimensional analysis of high-resolution X-ray computed tomography data with Morpho+. *Microsc*
729 *Microanal* 2011;17:252–63. doi:10.1017/S1431927610094389.
- 730 [62] Mendrik A, Vonken E -j., Witkamp T, Prokop M, van Ginneken B, Viergever M. Using the Fourth
731 Dimension to Distinguish Between Structures for Anisotropic Diffusion Filtering in 4D CT
732 Perfusion Scans. *Spat. Image Anal. Longitud. Time-Series Image Data*, Springer International
733 Publishing; 2015, p. 79–87.
- 734 [63] Mendrik A, Vonken EPA, Dankbaar JW, Prokop M, van Ginneken B. Noise filtering in thin-slice
735 4D cerebral CT perfusion scans. In: Benoit M. Dawant; David R. Haynor, editor. *SPIE Med.*
736 *Imaging Image Process.*, vol. 7623, San Diego: 2010, p. 76230N1–76230N8.
737 doi:10.1117/12.843813.
- 738 [64] Eklund A, Andersson M, Knutsson H. True 4D image denoising on the GPU. *Int J Biomed*
739 *Imaging* 2011;2011. doi:10.1155/2011/952819.
- 740 [65] Gal Y, Mehnert a J, Bradley a P, McMahon K, Kennedy D, Crozier S. Denoising of dynamic
741 contrast-enhanced MR images using dynamic nonlocal means. *IEEE Trans Med Imaging*
742 2010;29:302–10. doi:10.1109/TMI.2009.2026575.
- 743 [66] Kosior JC, Kosior RK, Frayne R. Robust dynamic susceptibility contrast MR perfusion using 4D
744 nonlinear noise filters. *J Magn Reson Imaging* 2007;26:1514–22. doi:10.1002/jmri.21219.
- 745 [67] Zitová B, Flusser J. Image registration methods: a survey. *Image Vis Comput* 2003;21:977–1000.
746 doi:10.1016/S0262-8856(03)00137-9.

- 747 [68] Latham S, Varslot T, Sheppard A. Image Registration : Enhancing and Calibrating X-Ray Micro-
748 Ct Imaging. Int. Symp. Soc. Core Anal., Abu Dhabi, UAE: Society of Core Analysts; 2008, p. 1-
749 12.
- 750 [69] Fife JL, Rappaz M, Pistone M, Celcer T, Mikuljan G, Stampanoni M. Development of a laser-
751 based heating system for in situ synchrotron-based X-ray tomographic microscopy. *J Synchrotron*
752 *Radiat* 2012;19:352–8. doi:10.1107/S0909049512003287.
- 753 [70] Chenouard N, Smal I, de Chaumont F, Maška M, Sbalzarini IF, Gong Y, et al. Objective
754 comparison of particle tracking methods. *Nat Methods* 2014;11:281–9. doi:10.1038/nmeth.2808.
- 755 [71] Maška M, Ulman V, Svoboda D, Matula P, Matula P, Ederra C, et al. A benchmark for
756 comparison of cell tracking algorithms. *Bioinformatics* 2014;30:1609–17.
757 doi:10.1093/bioinformatics/btu080.
- 758 [72] Coraluppi S, Carthel C. Multi-stage multiple-hypothesis tracking. *ISIF J Adv Inf Fusion*
759 2011;6:57–68.
- 760 [73] Chenouard N, Bloch I, Olivo-Marin JC. Multiple hypothesis tracking in microscopy images. *Proc -*
761 *2009 IEEE Int Symp Biomed Imaging From Nano to Macro, ISBI 2009*:1346–9.
762 doi:10.1109/ISBI.2009.5193314.
- 763 [74] Mader K. Quantitative big imaging: dynamic experiments 2014.
764 <https://raw.githubusercontent.com/kmader/Quantitative-Big-Imaging-Course/master/Lectures/09-Dynamic.pdf>
765 (accessed February 10, 2015).
- 766 [75] Bay BK, Smith TS, Fyhrie DP, Saad M. Digital volume correlation: Three-dimensional strain
767 mapping using X-ray tomography. *Exp Mech* 1999;39:217–26. doi:10.1007/BF02323555.
- 768 [76] Armstrong RT, Berg S. Interfacial velocities and capillary pressure gradients during Haines jumps.
769 *Phys Rev E* 2013;88:43010. doi:10.1103/PhysRevE.88.043010.
- 770 [77] Armstrong RT, Ott H, Georgiadis A, Rücker M, Schwing A, Berg S. Subsecond pore-scale
771 displacement processes and relaxation dynamics in multiphase flow. *Water Resour Res* 2014;n/a –
772 n/a. doi:10.1002/2014WR015858.
- 773 [78] Armstrong RT, Eyseev N, Koroteev D, Berg S. Interfacial velocities and the resulting velocity
774 field during a Haines jump. *Int. Symp. Soc. Core Anal., Avignon, France: Society of Core*
775 *Analysts*; 2014, p. 1–12.
- 776 [79] Dierick M, Van Loo D, Masschaele B, Van den Bulcke J, Van Acker J, Cnudde V, et al. Recent
777 micro-CT scanner developments at UGCT. *Nucl Instruments Methods Phys Res Sect B Beam*
778 *Interact with Mater Atoms* 2014;324:35–40. doi:10.1016/j.nimb.2013.10.051.
- 779 [80] Avraam DG, Payatakes AC. Flow Mechanisms, Relative Permeabilities, and Coupling Effects in
780 Steady-State Two-Phase Flow through Porous Media. The Case of Strong Wettability. *Ind Eng*
781 *Chem Res* 1999;38:778–86. doi:10.1021/ie980404o.

- 782 [81] Bultreys T, Boone MA, Boone MN, De Schryver T, Masschaele B, Hoorebeke L Van, et al. Real-
783 time visualization of Haines jumps in sandstone with laboratory-based micro-computed
784 tomography 2015;Submitted.
- 785 [82] Rolle M, Hochstetler D, Chiogna G, Kitanidis PK, Grathwohl P. Experimental Investigation and
786 Pore-Scale Modeling Interpretation of Compound-Specific Transverse Dispersion in Porous
787 Media. *Transp Porous Media* 2012;93:347–62. doi:10.1007/s11242-012-9953-8.
- 788 [83] Blunt MJ, Bijeljic B, Dong H, Gharbi O, Iglauer S, Mostaghimi P, et al. Pore-scale imaging and
789 modelling. *Adv Water Resour* 2013;51:197–216. doi:10.1016/j.advwatres.2012.03.003.
- 790 [84] Daccord G, Lenormand R, Liétard O. Chemical dissolution of a porous medium by a reactive
791 fluid-I. Model for the “wormholing” phenomenon. *Chem Eng Sci* 1993;48:169–78.
792 doi:10.1016/0009-2509(93)80293-Y.
- 793 [85] Gharbi O, Bijeljic B, Boek E, Blunt MJ. Changes in Pore Structure and Connectivity Induced by
794 CO₂ Injection in Carbonates: A Combined Pore-Scale Approach. *Energy Procedia* 2013;37:5367–
795 78. doi:10.1016/j.egypro.2013.06.455.
- 796 [86] Fourar M, Radilla G. Non-Fickian description of tracer transport through heterogeneous porous
797 media. *Transp Porous Media* 2009;80:561–79. doi:10.1007/s11242-009-9380-7.
- 798 [87] Ott H, Oedai S, Pentland CH, Linden a J Van Der. CO₂ Reactive Transport in Limestone : Flow
799 Regimes , Fluid Flow and Mechanical Rock Properties. *Int. Symp. Soc. Core Anal., Napa Valley,*
800 *USA: Society of Core Analysts; 2013, p. 1–12.*
- 801 [88] Koestel J, Larsbo M. Imaging and quantification of preferential solute transport in soil
802 macropores. *Water Resour Res* 2014;50:4357–78. doi:10.1002/2014WR015351.
- 803 [89] Clausnitzer V, Hopmans JW. Pore-scale measurements of solute breakthrough using microfocus
804 X-ray computed tomography. *Water Resour Res* 2000;36:2067. doi:10.1029/2000WR900076.
- 805 [90] Bijeljic B, Raeini A, Mostaghimi P, Blunt M. Predictions of non-Fickian solute transport in
806 different classes of porous media using direct simulation on pore-scale images. *Phys Rev E*
807 2013;87:013011. doi:10.1103/PhysRevE.87.013011.
- 808 [91] Ovaysi S, Piri M. Pore-scale modeling of dispersion in disordered porous media. *J Contam Hydrol*
809 2011;124:68–81. doi:10.1016/j.jconhyd.2011.02.004.
- 810 [92] Bultreys T, Van Hoorebeke L, Cnudde V. Multi-scale, micro-computed tomography-based pore
811 network models to simulate drainage in heterogeneous rocks. *Adv Water Resour* 2015;78:36–49.
812 doi:10.1016/j.advwatres.2015.02.003.
- 813 [93] Mehmani A, Prodanović M. The effect of microporosity on transport properties in porous media.
814 *Adv Water Resour* 2014;63:104–19. doi:10.1016/j.advwatres.2013.10.009.
- 815 [94] Roels S, Elsene J, Carmeliet J, Hens H. Characterisation of pore structure by combining mercury
816 porosimetry and micrography. *Mater Struct* 2001;34:76–82.